Non-commutative tomography: A tool for data analysis and signal processing

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> > October 2011

- Integral transforms: linear and bilinear
- Wavelet-type, quasi-distributions and tomograms: Examples and relations
- Tomograms and the conformal group operators
- Aplications:
- Detection of small signals
- Iltering and component separation
- Plasma reflectometry

• Integral transforms

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• 1 - Wavelet-type transform

$$W_{f}^{(h)}(\alpha) = \langle U(\alpha) h | f \rangle,$$

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• 3 - Tomographic transform or tomogram

$$M_{f}^{(B)}(X) = \langle f \mid \delta \left(B \left(\alpha \right) - X \right) \mid f \rangle$$

• Fourier transform: is $W_f^{(h)}(\alpha)$ if $U(\alpha)$ is unitary generated by $B_F(\overrightarrow{\alpha}) = \alpha_1 t + i\alpha_2 \frac{d}{dt}$ and *h* is a (generalized) eigenvector of the time-translation operator

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- Bertrand transform: $Q_f(\alpha)$ for B_W

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• The tomogram is a homogeneous function

$$M_{f}^{(B/p)}(X) = |p| M_{f}^{(B)}(pX)$$

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$$| f_1 \rangle = | h \rangle + | f \rangle; \qquad | f_3 \rangle = | h \rangle - | f \rangle; | f_2 \rangle = | h \rangle + i | f \rangle; \qquad | f_4 \rangle = | h \rangle - i | f \rangle.$$

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• Quasidistribution of the Husimi-Kano type

$$H_f^{(b)}(\alpha) = \langle f \mid U(\alpha) \mid f \rangle.$$

The conformal group

• The generators of the conformal group

$$\begin{array}{ll} \text{in } \mathbb{R}^d & \omega_k = i \frac{\partial}{\partial t_k} \\ D = i \left(t \bullet \nabla + \frac{d}{2} \right) \\ R_{j,k} = i \left(t_j \frac{\partial}{\partial t_k} - t_k \frac{\partial}{\partial t_j} \right) \\ K_j = i \left(t_j^2 \frac{\partial}{\partial t_j} + t_j \right) \end{array}$$

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• For *d* = 1

in ${\mathbb R}$

$$\begin{split} \omega &= i \frac{d}{dt} \\ D &= i \left(t \frac{d}{dt} + \frac{1}{2} \right) \\ \mathcal{K} &= i \left(t^2 \frac{d}{dt} + t \right) \end{split}$$

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Time-conformal

$$B_4 = \mu t + i\nu \left(t^2 \frac{d}{dt} + t \right)$$

• General construction of the tomograms: Let

$$\int dY \ket{Y}ig Y = 1$$

be a decomposition of the unit, with generalized eigenvectors of the operator B. Then

$$M(\alpha, X) = \int dY \langle f \mid \delta (B(\alpha) - X) \mid Y \rangle \langle Y \mid | f \rangle = |\langle X \mid f \rangle|^{2}$$

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- $B_1\psi_1(\mu,\nu,t,X) = X\psi_1(\mu,\nu,t,X)$

$$\psi_1(\mu,\nu,t,X) = \exp i\left(\frac{\mu t^2}{2\nu} - \frac{tX}{\nu}\right)$$

$$\int dt \psi_1^*\left(\mu,\nu,t,X\right)\psi_1\left(\mu,\nu,t,X'\right) = 2\pi\nu\delta\left(X-X'\right)$$

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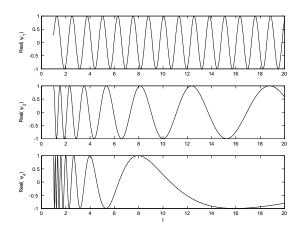
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• $B_4\psi_4(\mu, \nu, t, X) = X\psi_4(\mu, \nu, t, X)$
 $\psi_4(\mu, \nu, t, X) = \frac{1}{|t|}\exp i\left(\frac{X}{\nu t} + \frac{\mu}{\nu}\log|t|\right)$
 $\int dt\psi_4^*(\mu, \nu, t, s)\psi_4(\mu, \nu, t, s') = 2\pi\nu\delta(s - s')$

RVM (IPFN)

 $\mu = 0$



• Time-frequency tomogram

$$M_1(\mu,\nu,X) = \frac{1}{2\pi|\nu|} \left| \int \exp\left[\frac{i\mu t^2}{2\nu} - \frac{itX}{\nu}\right] f(t) dt \right|^2$$

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Frequency-scale tomogram

$$M_{3}(\mu,\nu,X) = \frac{1}{2\pi|\nu|} \left| \int d\omega \frac{f(\omega)}{\sqrt{|\omega|}} e^{\left[-i\left(\frac{\mu}{\nu}\omega - \frac{X}{\nu}\log|\omega|\right)\right]} \right|^{2}$$
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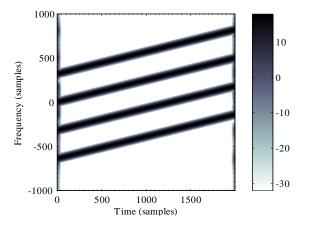
 $f(\omega) =$ Fourier transform of f(t)

• Time-conformal tomogram

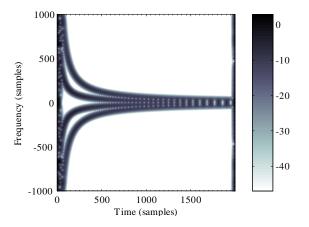
$$M_4(\mu,\nu,X) = \frac{1}{2\pi|\nu|} \left| \int dt \, \frac{f(t)}{|t|} e^{\left[i\left(\frac{X}{\nu t} + \frac{\mu}{\nu}\log|t|\right)\right]} \right|^2$$

RVM (IPFN)

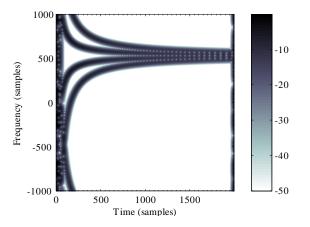
Time-frequency



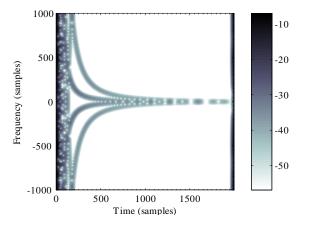
Time-scale



Time-scale



Time-conformal



• 1 - Detection of small signals in noise

Image: A math a math

- 1 Detection of small signals in noise
- Let in $M_1(\mu, \nu; X)$ $\mu = \frac{\cos \theta}{T}, \nu = \frac{\sin \theta}{\Omega}$

(Radon transform)

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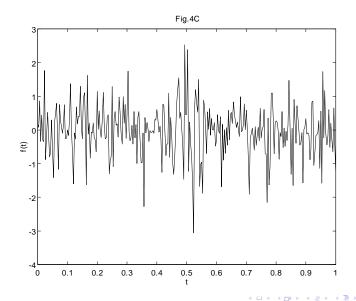
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 A signal generated as a superposition of a normally distributed random amplitude - random phase noise with a sinusoidal signal of same average amplitude, operating only during the time 0.45 - 0.55. The signal to noise power ratio is 1/10.

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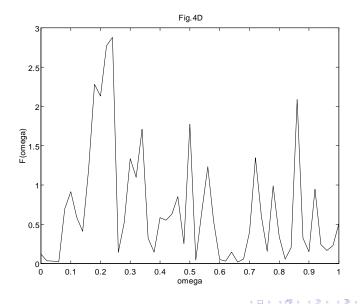
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- The. following figures show the signal, its Fourier transform and the tomogram $M_f^{(S)}(s, \mu, \nu)$ (T = 1 and $\Omega = 1000$)

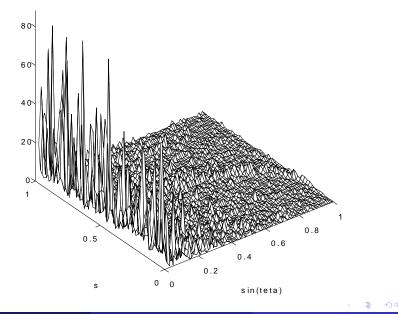


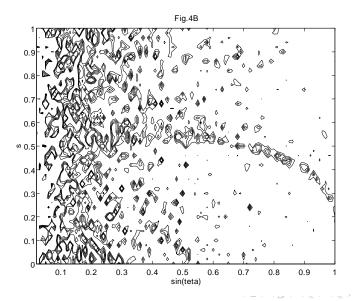
RVM (IPFN)

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RVM (IPFN)





RVM (IPFN)

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- A ridge of small peaks is reliable because the rigorous probability interpretation of $M(\theta, X)$ renders the method immune to spurious effects.

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- One possibility: Separation of components using its behavior in the time-frequency plane. Consider the finite-time tomogram

$$M(\theta, X) = \left| \int f(t) \psi_{\theta, X}(t) dt \right|^2 = \left| \langle f, \psi \rangle \right|^2$$

with

$$\psi_{\theta,X}(t) = \frac{1}{\sqrt{T}} \exp\left(\frac{-i\cos\theta}{2\sin\theta} t^2 + \frac{iX}{\sin\theta} t\right)$$

 $\mu = \cos \theta$, $\nu = \sin \theta$.

RVM (IPFN)

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- θ is a parameter that interpolates between the time and the frequency operators, running from 0 to $\pi/2$ whereas X is allowed to be any real number.
- For all different θ 's the $U(\theta)$ are unitarily equivalent operators, hence all the tomograms share the same information. The component separation technique is based on the search for an intermediate value of θ where a good compromise might be found between time localization and frequency information.
- First select a subset X_n in such a way that the corresponding family $\left\{\psi_{\theta,X_n}(t)\right\}$ is orthogonal and normalized,

$$<\psi_{\theta,X_n}\psi_{\theta,X_m}>=\delta_{m,n}$$

This is possible by taking the sequence

$$X_n = X_0 + \frac{2n\pi}{T}\sin\theta$$

where X_0 is freely chosen (in general we take $X_0 = 0$)

• We then consider the projections of the signal f(t)

$$c^ heta_{X_n}(f) = < f$$
 , $\psi_{ heta,X_n} >$

which are used for the signal processing.

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• Denoising consists in eliminating the $c_{X_a}^{\theta}(f)$ such that

$$\left|c_{X_n}^{\theta}(f)\right|^2 \leq \epsilon$$

for some threshold ϵ

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• Multi-component analysis is done by selecting subsets \mathcal{F}_k of the X_n and reconstructing partial signals (k-components) by restricting the sum to

$$f_k(t) = \sum_{n \in \mathcal{F}_k} c^ heta_{X_n}(f) \psi_{ heta, X_n}(t)$$

for each k.

Component decomposition. Examples

 $y(t) = y_1(t) + y_2(t) + y_3(t) + b(t)$ $y_1(t) = \exp(i25t), t \in [0, 20]$ $y_2(t) = \exp(i75t), t \in [0, 5]$ $y_3(t) = \exp(i75t), t \in [10, 20]$

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Component decomposition. Examples

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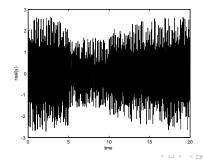
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• Real part of the time signal



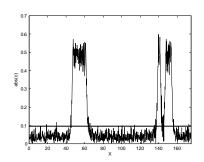
• Separation at $\theta = \frac{\pi}{5}$

Component decomposition. Examples

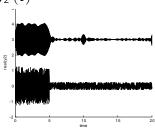
• Separation at $\theta = \frac{\pi}{5}$

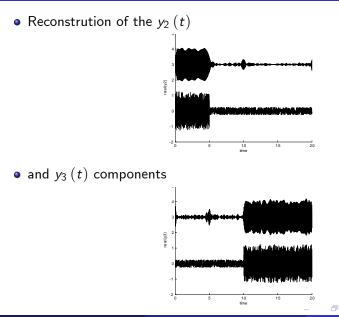
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• Reconstrution of the $y_2(t)$





RVM (IPFN)

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• Sum $y(t) = y_0(t) + y_R(t) + b(t)$ of an "incident" $y_0(t)$ and a "deformed reflected" chirp $y_R(t)$ delayed by 3s with white noise added.

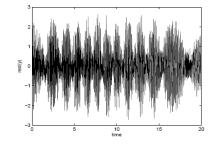
$$y_0(t) = e^{i\Phi_0(t)}$$
 $y_R(t) = e^{i\Phi_R(t)}$

 $\Phi_0(t) = a_0 t^2 + b_0 t \text{ and}$ $\Phi_R(t) = a_R (t - t_R)^2 + b_R (t - t_R) + 10(t - t_R)^{\frac{3}{2}}.$

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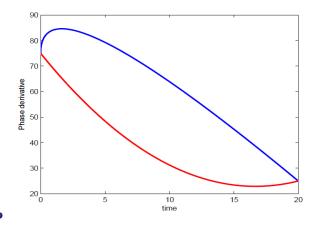
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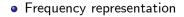


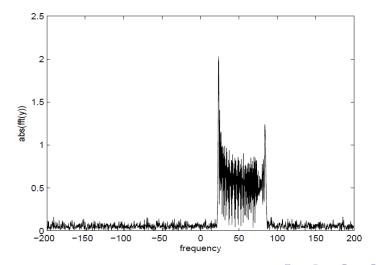
RVM (IPFN)

• Comparison of the phase derivatives $\frac{d}{dt}\Phi_0(t)$ and $\frac{d}{dt}\Phi_R(t)$. Except for the three first seconds, the spectrum of the signals $y_0(t)$ and $y_R(t)$ is almost the same

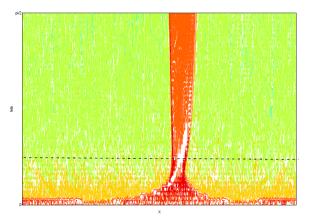
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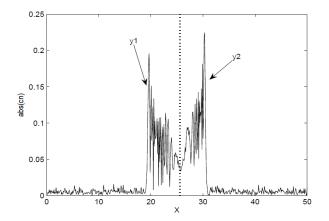




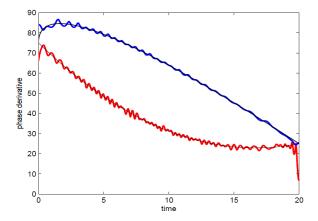
• Tomogram of the chirps signal



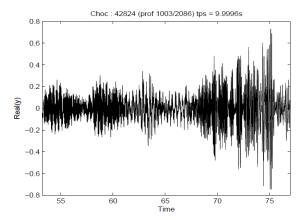
Separable spectrum at $\theta = \frac{\pi}{5}$

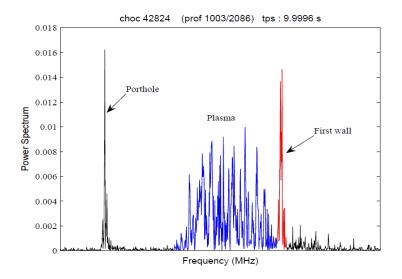


The phase derivative

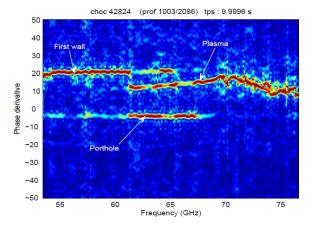


Reflectometry signal

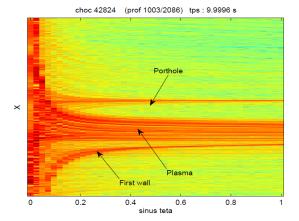




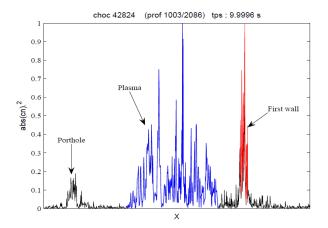
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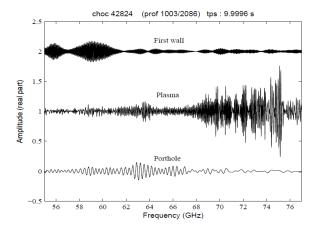


• Tomogram of the reflectometry signal



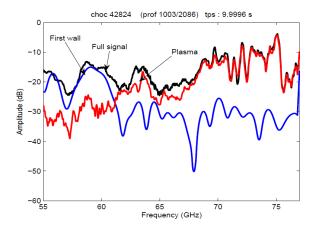
• "Spectrum" at $\theta = \pi - \frac{\pi}{5}$

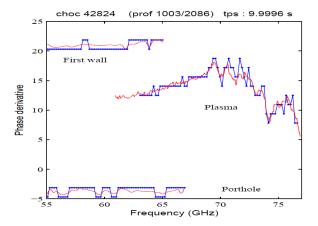




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Image: Image:





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 RVM (IPFN)